Life After Death:

Techniques for the rapid prognostication of post-anoxic coma patients.

Mohammad M. Ghassemi Massachusetts Institute of Technology

Cardiac arrest affects 320K people in the US annually



[4] G. Citerio, J. Bakker, M. Bassetti, D. Benoit, M. Cecconi, J. Curtis, G. Doig, M. Herridge, S. Jaber, and M. Joannidis, "Year in review in intensive care medicine 2014: I. cardiac dysfunction and cardiac arrest, ultrasound, neurocritical care, icu-acquired weakness, nutrition, acute kidney injury, and miscellaneous," *Intensive Care Medicine*, vol. 41, no. 2, pp. 179–191, 2015.

128K patients are successfully resuscitated



[5] K. Kern, "Optimal treatment of patients surviving out-of-hospital cardiac arrest," JACC: Cardiovascular Interventions, vol. 5, no. 6, pp. 597–605, 2012.

100K enter an indefinite, anoxia-induced coma



[6] R. Deng, M. Koenig, L. Young, and X. Jia, "Early quantitative gamma-band eeg marker is associated with outcomes after cardiac arrest and targeted temperature management," *Neurocritical Care*, vol. 23, no. 2, pp. 262–273, 2015.

10K will survive, but only 5K will regain normal function



[7] P. R. L. I. for Health Policy, "Icu outcomes (mortality and length of stay) methods, data collection tool and data." http://healthpolicy.ucsf.edu/content/icu-outcomes, 2016.

Outcome_metric

Cerebral Performance Category	$\begin{array}{c} \text{Conscious} \\ (\text{Y/N}) \end{array}$	Cerebral Disability	Consequences
1	Υ	Mild	May resume independent activities with minimal complications
2	Y	Moderate	May resume independent activities while requiring some assistance
3	Y	Severe	Will require assistance to perform activities and may involve paralysis, or dementia.
4	Ν	Vegetative	Requires assistance to survive and will be minimally aware/responsive
5	Ν	Brain-Death	Requires assistance to survive and will be totally unaware/response

Outcome_metric

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	2	Υ	Moderate	May resume independent activities while requiring some assistance	
	3	Υ	Severe	Will require assistance to perform activities and may involve paralysis, or dementia.	
	4	Ν	Vegetative	Requires assistance to survive and will be minimally aware/responsive	Bad
	5	Ν	Brain-Death	Requires assistance to survive and will be totally unaware/response	

Goals of prognostication

- **Primary:** Prevent premature withdrawal care
- Secondary: Prevent unnecessary care (up to \$20,000 per day in ICU)

Current Prognostic Guidelines

- A sequence of clinical observations and tests performed following cardiac arrest
- Accurate in predicting poor neurological outcomes when severe deficits are present (FPR < 1%)
- Less guidance in cases where clear-cut signs are lacking, or under varying protocols (e.g. therapeutic hypothermia)



The American Academy of Neurology

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The American Academy of Neurology

EEG Features Tjepkema-Cloostermans, 2017 AUC = 0.94 at 24 hours N = 283

Pain-related SSEP Zanatta, 2015 AUC = 0.84 at 72 hours N = 167

NSE Dagmar, 2017 AUC = 0.77 at 24 hours N = 153



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Conclusions

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- **Time Specific:** prediction should be possible at all points in time

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- Classification focused: risk scoring may be better

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- EEG alone can provide state-of-the-art performance

Conclusions

- Limited Sample Sizes: larger samples are needed
- Time Specific: prediction should be possible at all points in time
- Classification focused: risk scoring may be better
- EEG alone can provide state-of-the-art performance
 - deep learning could eliminate the need for feature engineering



1. 'Bigger' data sets

2. Time-sensitive



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Data collection



1. 'Bigger' data sets **2.** Time-sensitive

Electroencephalography (EEG)

- Each EEG electrode records an **ensemble** of cellular activity near the location of the electrode
- Electrode Placement was in accordance with the International 10-20 system

Electrodes Brain EEG reading

Electroencephalogram (EEG)

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Electroencephalogram (EEG)

- 5 contributing institutions
- 785 unique patients
- 7 terabytes of data



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- 5 contributing institutions
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- Over 2x larger than existing archives described in the literature



EEG temporal properties

- Data densities linearly decrease over time
- EEG withdrawal is assessed approximately once every 24 hours



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Chillean Eature (Mean)	Good Outcomes	Bad Outcomes
Age (Years)	57	63
Gender (% Male)	68	68
ROSC (Mins)	19.47	25.7
Rhythm at Arrest (%)		
VFib	69	34
Other (PEA / Asystole)	25	61
Unknown	6	5
Cause of Arrest (%)		
Pulmonary	50	34
Anesthesia	3.6	8.5
Neurologic	9.6	13.8
Other/Unknown (%)	36.8	43.7
Arrest Location		
In Hospital (%)	9	11
Out of Hospital (%)	63	56
Unknown (%)	28	33

- Average Age: 60
- Older patients do worse



Clinical Feature (Mean)	Good Outcomes	Bad Outcomes
Age (Years)	57	63
Unknown (%)	28	33

- 68% Male
- No difference w.r.t. outcome



Clinical Feature (Mean)	Good Outcomes	Bad Outcomes
Age (Years)	57	63
Gender (% Male)	68	68
Unknown (%)	28	33

- Average ROSC time: 23 mins
- Longer time to ROSC is bad



Clinical Feature (Mean)	Good Outcomes	Bad Outcomes
Age (Years)	57	63
Time to ROSC (Mins)	19.47	25.7
Unknown (%)	28	33

- 50% have Vfib arrest rhythm
- VFib patients do better



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Causes are often unknown



Clinical Feature (Mean)	Good Outcomes	Bad Outcomes
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- Location often unknown
- Most are outside hops.



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Arrest Location		
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Data Collection



1. 'Bigger' data sets2. Time-sensitive

3. Deployable

Data Collection



1. Collected an EEG archive 2x larger than largest set previously described in the literature

Time-sensitive

3. Deployable

Develop time-sensitive modeling approaches



 Collected an EEG archive 2x larger than largest set previously described in the literature 2. Time-sensitive

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Three Approaches

Two Feature Based:

- 1. Sequential Logistic Regression with 'Elastic' memories.
- 2. Sequential Logistic Regression with Dynamic Bayesian network constraints

One Data Driven

• 3. Deep neural networks

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2. Identify artifacts in five second epochs

- 2.1 Disconnects and saturation
- 2.2 Eye and muscle artifact
- 2.3 Moment-based artifacts



- 3. Choose five minute epochs with minimal artifact
 - 3.1 Generate artifact score
 - 3.2 Identify cleanest epochs in each hour of data





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• Complexity (21 features)

• Category (31 features)

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F3-C3	nAn
C3-P3 May May May May May May May May May May	M
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F4-C4	m
C4-P4	m
P4-02	, ~~
Fp1-F7	m
F7-T3	$\sim \sim \sim \sim$
T3-T5 mm	\sim
T5- <u>01</u>	
Fp2-F8	\sim
F8-T4	~~
T4-T6	m
T6-02-	m
Fz-Cz	~^~
Cz-Pz	m
11 12 13 14 15 16 17 18 19 Time (seconds)	20

- Complexity (21 features)
 e.g. Shannon Entropy
- Category (31 features)

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Fp1-F7			www.www			
T5- <u>01</u>						
Fp2-F8 F8-T4		Les	s comp	lex		
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 e.g. Burst Suppression
- Connectivity (7 features)



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• Connectivity (7 features) e.g. cross correlation



The mean and standard error of three features for the study population, partitioned by outcome



Shannon Entropy (a measure of complexity) distinguishes 'Good' and 'Bad' consistently









Regularity (a measure of burst-suppression) distinguishes 'Good' and 'Bad' earlier







Cross correlation (a measure of complexity) distinguishes 'Good' and 'Bad' later



Conclusion

- The features-outcome relationship changes over time
- Needs modelling approach where coefficients evolve over time

Three Approaches

Two Feature Based:

- 1. Sequential Logistic Regression with 'Elastic' memories
- 2. Sequential Logistic Regression with Dynamic Bayesian network constraints

One Data Driven

• 3. Deep neural networks
• n = 438 patients

• We used 52/57 features

• Validation: 10-fold



- We train a series of models that classify patient outcomes, in particular time intervals:
 - 1-12 hours 13-24 hours 25-36 hours etc.



Time (Hours)

- Features are extracted at particular time intervals
- 1-12 hours



Time (Hours)

- Features are extracted at particular time intervals
- 13-24 hours



- Features are extracted at particular time intervals
- 25-36 hours, and so on...



 Features used by models in earlier time intervals are passed forward as 'memories' for models in future time intervals



Time (Hours)

 Features used by models in earlier time intervals are passed forward as 'memories' for models in future time intervals



 Features used by models in earlier time intervals are passed forward as 'memories' for models in future time intervals



10%

- We retain only the most important features using Elastic Net
- Penalizes the size of the regression coefficients based on both their *l*¹ norm and their *l*² norm :

$$argmax_{\beta}\sum_{i}\log L(y_{i};\beta,x_{i})-\lambda[\alpha||\beta||_{1}+\frac{1}{2}(1-\alpha)||\beta||_{2}^{2}]$$

Extract features 1-12 Hrs From training set 13-24 Hrs 25-36 Hrs features features train features 90% Elastic Elastic Elastic Net Net Net Identify features predictive within time interval test 10%

Time (Hours)

 A logistic regression model with the selected features is used to evaluate performance on the held out test-sets



- A logistic regression model with the selected features is used to evaluate performance on the held out test-sets
- This process was designed to imitate how providers might perform prognosis



Coefficients Mat Reflect Three Kinds of Relationships

- An **immediate value** is most predictive of outcomes.
- A prior value is most predictive of outcomes.
- The **cumulative** value is most predictive of outcomes.













- Our approach exhibited enhanced calibration compared to the literature baseline
- This allows for a more nuanced use of the model, compared to existing approaches



• Our approach was also well calibrated over time.



• Our approach was also well calibrated over time.





- Our approach was also well calibrated over time.
- Day 2



- Our approach was also well calibrated over time.
- Day 3



• Our approach was also well calibrated over time.



1-24 hours 25 - 48 hours 49 - 72 hours

Calibration







0-12 Hours 13-24 Hours 37-48 Hours 49-60 Hours 61-72 Hours 25-36 Hours and a second and the second ngahalulan pantipapan akambahah pantahan - menerandan munitur ana kabahan kabahan kabahan kabahan kabahan kabah 85% 95% 83% 80% 78% CPC 1 mothersensers was an and a subman and a subman and a subman subman and a subman and a subman and a subman and a appenanter and the second of t 80% 80% 90% 93% 50 Hz 83% 79% CPC 2 25 Hz 0 Hz man man when we we we we we wanter and the second s 50 Hz 53% 58% 60% 54% 53% 52% CPC 3 25 Hz 0 Hz MAMM - Amarkan from 15 mm 13% 10% 22% 10% 19% CPC 4 **Power/Frequency** (dB/Hz) mm my mullim 2% 3% 2% 3% 1% CPC 5 -25 10 Seconds **10 Seconds 10 Seconds 10 Seconds** 10 Seconds

















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Pros/Cons of the Approach

- Advantages
 - Does not require time of arrest
 - Prognostic performance improves over time using 'memories'
 - Well calibrated
- Disadvantages
 - Alignment with respect to EEG initiation harm physiological interpretations
 - Assumes that feature coefficients in neighboring intervals are independent
 - Does not account for spatial information

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- n = 785 patients
- 10 EEG, 5 clinical features
- Validation:
- Leave-one-subject-out

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Signal Feature Complexity Shannon Entropy Hjorth Complexity False Nearest Neighbor Category Standard Deviation Regularity (burst-suppression) Diffuse Slowing Spikes Connectivity Coherence - delta Phase Lag Index Cross-correlation Magnitude

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• We extracted features in 12 hour intervals:



- We extracted features in 12 hour intervals:
- 1-12 hours



- We extracted features in 12 hour intervals:
- 13-24 hours



Time (Hours)

- We extracted features in 12 hour intervals:
- 25-36 hours



- We extracted features in 12 hour intervals:
- etc...



- We learn parameters of several logistic regressions: *coefficient measures* β_i^j
- With corresponding *coefficient* measure errors R_i^j , which are simply the standard errors



 To relate the coefficient measurements across time intervals, we specify a model of coefficient dynamics which provide *coefficient estimates* βⁱ_i

$$f(\beta_i^{j-1}) = \beta_i^{j-1} + \Delta(\beta_i^{j-1}) = \bar{\beta}_i^j$$

• With estimate error denoted by $\bar{P_i^j}$

 $\bar{P_i^j} = P_i^{j-1} + Q$



$$\bar{\beta}_i^j$$

• A simple DBN (the kalman filter) recursively determine the optimal coefficient estimates

$$\beta_i^j = \bar{\beta}_i^j + K_i^j [\tilde{\beta}_i^j - \bar{\beta}_i^j],$$
$$K_{(i,j)} = \frac{\bar{P}_i^j}{\bar{P}_i^j + R_i^j}$$

• With coefficient uncertainty

$$P_i^j = (1 - K_i^j) \bar{P}_i^{j-1}$$



• DBN estimates rely more strongly on prior estimates when present estimates have high standard error



Results

The Sequential Logistic Regression with DBN had the best overall prognostic performance when compared to several baseline approaches.

Model	Features	Temporal	AUC	\mathbf{TPR}	\mathbf{TPR}
		Assumptions		FPR=0.05	FPR=0.01
Logistic Regression	5 Clinical, 10 EEG	Kalman Filter	0.86	0.49	0.29
Logistic Regression	5 Clinical, 10 EEG	Independent	0.84	0.46	0.26
Logistic Regression	10 EEG	Kalman Filter	0.83	0.47	0.25
Random Forest	5 EEG [2]	Independent	0.82	0.44	0.21
Logistic Regression	10 EEG	Independent	0.81	0.44	0.19
Logistic Regression	5 Clinical	None	0.73	0.26	0.11

Results over time

- The DBN approach had the best performance over time (peak AUC: 0.87)
- performance decreases over time (min AUC: 0.84)



Calibration

- The DBN approach was the best calibrated of the tested approaches
- The direction of mis-calibration was 'optimistic', tending to over-estimate 'good' outcomes.



Model coefficients evolve over time in a sensible way, and are interpretable.



Entropy 1 std above the mean at 12 hours \rightarrow 0.33 times as likely to have a bad outcome



Entropy 1 std above the mean at 48 hours \rightarrow 0.5 times as likely to have a bad outcome



Epileptiforms 1 std below the mean at 12 hours \rightarrow 1.1 times as likely to have a bad outcome



Epileptiforms 1 std below the mean at 48 hours \rightarrow 2.2 times as likely to have a bad outcome



PLI 1 std below the mean at 12 hours \rightarrow 1.5 times as likely to have a bad outcome



PLI 1 std below the mean at 48 hours \rightarrow 3 times as likely to have a bad outcome



Pros/Cons of the Approach

- Advantages
 - Features are lightweight: 10 in total
 - Model is interpretable and may aid providers without formal deployment
 - Excellent LOOCV prognostication performance relative to baselines
- Disadvantages
 - Without 'memories', performance decreases over time
 - Possibility that important features were overlooked
 - Does not account for spatial information

Three Approaches

Feature Based:

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2. Sequential Logistic Regression with Dynamic Bayesian network constraints

Data Driven

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Limitations of the feature-based approaches

- Requires thoughtful pre-processing pipeline
- Requires computation of features
- By averaging over channels, features eliminate spatial information
- Possibility that certain features might have been missed

Motivation

 Even if all 57 features were used, derivatives of features may be useful features



Motivation

 Deep Neural Networks provide an potential solution to this problem because they derive features from the data automatically



- n = 724 patients
- 4 topographic energy plots: [0-3, 4-7, 8-15, 16-31] Hz
- Pseudo-subject generation
- Validation: Leave-one-institution-out

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Band

δ [0 - 3 Hz]

Θ

СL

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- Validation:
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-20db -- 10db



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Band

δ

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- 300 topologies were tested
- 100, 2 Dimensional Convolutional Neural Networks
- 100, 3 Dimensional Convolutional Neural Networks
- 100, Long-term Recurrent Convolutional Networks

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Source: http://alifar76.github.io/cnn-microbiome/

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- 100, Long-term Recurrent
 Convolutional Networks



• 3D CNNs provide performance on par with the bestperforming feature-based approaches.

	AUROC	TPR FPR=0	TPR FPR=1%	TPR FPR=5%
Neural Networks				
2D CNN	0.71(0.09)	0(0.0)	0.09(0.06)	0.23(0.10)
**3D CNN	0.81(0.04)	0.24(0.05)	0.30(0.05)	0.45(0.09)
LRCN	0.79(0.08)	0.19(0.11)	0.34~(0.15)	0.48~(0.15)
\mathbf{SVM}				
*Linear	0.76(0.13)	0.17(0.18)	$0.21 \ (0.16)$	0.32(0.19)
Quadratic	0.72(0.14)	0.14(0.09)	0.16(0.09)	0.26(0.12)
Fine Gaussian	0.75(0.14)	0.18(0.14)	0.2(0.12)	0.31~(0.19)
Medium Gaussian	0.56~(0.03)	$0.01 \ (0.02)$	$0.01 \ (0.02)$	0.06(0.04)
Coarse Gaussian	0.71 (0.13)	0.07~(0.12)	0.08(0.12)	0.15~(0.1)
Discriminant Analysis				
Linear	0.77~(0.15)	$0.21 \ (0.13)$	0.23~(0.14)	0.34~(0.25)
* Quadratic	0.78(0.14)	$0.22 \ (0.13)$	0.25~(0.14)	0.4(0.22)
Cubic	0.72(0.13)	0 (0)	0 (0)	0.15~(0.24)
Decision Trees				
Simple	0.68(0.11)	0 (0)	0 (0)	0 (0)
Medium	0.7~(0.09)	0.05~(0.11)	0.05~(0.11)	$0.11 \ (0.16)$
Complex	0.69(0.07)	0 (0)	0 (0)	0 (0)
*RUS Boosted	0.8(0.1)	0.25~(0.2)	0.25~(0.2)	0.39(0.17)
Ensemble Boosted	0.74(0.12)	0.12(0.17)	0.12(0.17)	0.14(0.19)
Ensemble Bagged	0.77~(0.1)	0.09(0.14)	$0.11 \ (0.13)$	0.22~(0.15)

• 3D CNNs provide performance on par with the bestperforming feature-based approaches.

	AUROC	TPR FPR=0	$\begin{array}{c} \text{TPR} \\ \text{FPR}=1\% \end{array}$	$\begin{array}{c} \text{TPR} \\ \text{FPR} = 5\% \end{array}$
Neural Networks				
2D CNN	0.71(0.09)	0(0.0)	0.09(0.06)	0.23(0.10)
**3D CNN		0.24(0.05)	0.30(0.05)	0.45(0.09)
LRCN	0.79(0.08)	0.19 (0.11)	0.34(0.15)	0.48(0.15)
\mathbf{SVM}				
*Linear	0.76(0.13)	0.17(0.18)	$0.21 \ (0.16)$	0.32(0.19)
Quadratic	0.72(0.14)	0.14(0.09)	0.16(0.09)	0.26(0.12)
Fine Gaussian	0.75~(0.14)	0.18(0.14)	0.2(0.12)	$0.31 \ (0.19)$
Medium Gaussian	0.56~(0.03)	$0.01 \ (0.02)$	$0.01 \ (0.02)$	0.06(0.04)
Coarse Gaussian	$0.71 \ (0.13)$	0.07~(0.12)	0.08(0.12)	0.15(0.1)
Discriminant Analysis				
Linear	0.77~(0.15)	$0.21 \ (0.13)$	0.23~(0.14)	0.34~(0.25)
*Quadratic	0.78(0.14)	0.22(0.13)	0.25~(0.14)	0.4(0.22)
Cubic	0.72~(0.13)	0(0)	0(0)	0.15~(0.24)
Decision Trees				
Simple	0.68(0.11)	0 (0)	0(0)	0(0)
Medium	0.7(0.09)	0.05~(0.11)	0.05(0.11)	0.11 (0.16)
Complex	0.69(0.07)	0 (0)	0(0)	0 (0)
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Pros/Cons of the Approach

- Advantages
 - No feature engineering
 - No pre-processing required
 - Performance is on par with, or exceeds, feature-based approaches
- Disadvantages
 - Requires 72 hours of data
 - Requires tuning of 300K+ parameters
 - Models are difficult to interpret

Develop time-sensitive modeling approaches



1. Collected an EEG archive 2x larger than largest set previously described in the literature 2. Time-sensitive

Develop *time-sensitive* modeling approaches



- Collected an EEG archive 2x larger than largest set previously described in the literature
- 2. Demonstrated 3 time-sensitive approaches that out-perform state-of-the-art

Choosing a model for deployment



- Collected an EEG archive 2x larger than largest set previously described in the literature
- 2. Demonstrated 3 time-sensitive approaches that out-perform state-of-the-art

Criteria for deployment

- Interpretable
 - Clear why model has provided the prognostication at hand
- Robust
 - Robust to issues of missing data (e.g. lost channels)
- Well-calibrated
 - Accurate mapping between predicted and actual probabilities of outcome

Proposed model for deployment: sequential logistic regression with DBN constraints



Hours Since Cardiac Arrest

Choosing a model for deployment



- Collected an EEG archive 2x larger than largest set previously described in the literature
- 2. Demonstrated 3 time-sensitive approaches that out-perform state-of-the-art

Assessing performance: classification and calibration



- Collected an EEG archive 2x larger than largest set previously described in the literature
- 2. Demonstrated 3 time-sensitive approaches that out-perform state-of-the-art

3. Our proposed approach provides excellent classification, is well-calibrated, and Interpretable

Summary

Collected 785 PAC patients from five university affiliated hospitals

- 35,000 hours of 21-channel continuous EEG recordings,
- A selection of clinical covariates and an ordinal measure of

Extracted 57 quantitative EEG features that capture three signal properties

- Complexity: the degree of randomness in the EEG signal,
- Category: qualitative descriptors of signal characteristics or behaviours and
- Connectivity: interactions between EEG electrodes.

Tested novel methods for time-sensitive classification of outcomes

- Penalized, sequential, logistic regression using 57 multi-scale features,
- Logistic regression using 10 qEEG features constrained by a DBN and
- A variety of deep neural network architectures

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Contributors: Edilberto Amorim Tuka Alhanai Jong Woo Lee Michel van Putten Jeannette Hofmeijer Adithya Sivaraju Nicolas Gaspard Barry Ruijter Siddharth Biswal Valdery Moura Junior Michael Donnino Susan Herman

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Dr. M. Brandon Westover

Prof. Thomas Heldt



Time Domain Characteristics Frequency Domain Characteristics 20 Category Ηz when when the second and the second and the second se Low Voltage 0 20 Normal Hz 0 20 Diffuse Th Hz Slow 0 20 Epileptiform when how the Hz WM 0 20 Burst Ηz Suppresion 0 15 0 10 -25 Time (Seconds) Power/Frequency (dB/Hz)
Connectivity



Less Connectivity

Estimated Connectivity Of Signals

More Connectivity